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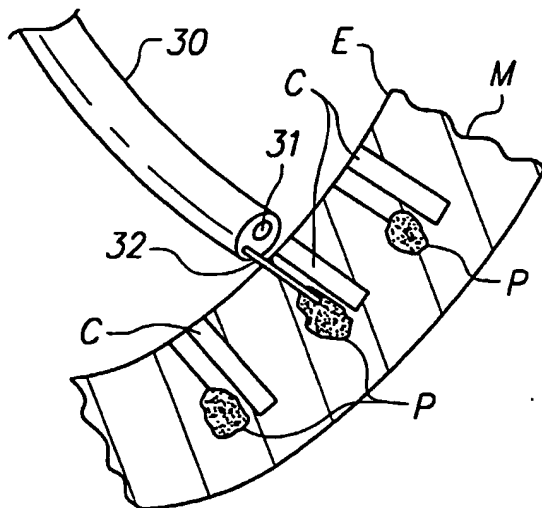
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For two-letter codes and other abbreviations, refer to the "Guidance Notes on Codes and Abbreviations" appearing at the beginning of each regular issue of the PCT Gazette.

(54) Title: APPARATUS AND METHODS FOR PERFORMING PERCUTANEOUS MYOCARDIAL REVASCULARIZATION AND STIMULATING ANGIOGENESIS USING AUTOLOGOUS MATERIALS



(57) Abstract: Methods are provided for collecting, and processing autologous biological materials to form autologous angiogenic agents. Apparatus (30), and methods also are provided for performing percutaneous myocardial re-vascularization wherein an injection needle (32) is disposed in spaced-apart relation to the channel forming tool (31) so that a predetermined amount of the autologous angiogenic agent may be injected into the myocardium (M) adjacent to the PMR channel (C).

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APPARATUS AND METHODS FOR PERFORMING PERCUTANEOUS  
MYOCARDIAL REVASCULARIZATION AND STIMULATING  
ANGIOGENESIS USING AUTOLOGOUS MATERIALS

Field Of The Invention

5           The present invention relates to apparatus  
and methods for performing percutaneous myocardial  
revascularization and injecting autologous materials  
into the treated tissue to stimulate angiogenesis.

Background Of The Invention

10           A leading cause of death in the United States  
today is coronary artery disease, in which  
atherosclerotic plaque causes blockages in the coronary  
arteries, resulting in ischemia of the heart (i.e.,  
inadequate blood flow to the myocardium). The disease  
15 manifests itself as chest pain or angina. In 1996,  
approximately 7 million people suffered from angina in  
the United States.

          One technique that has been developed to  
treat patients suffering from diffuse atherosclerosis,  
20 is referred to as percutaneous myocardial

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5     revascularization (PMR). In this method, a series of  
channels are formed in the left ventricular wall of the  
heart extending inward from the myocardium. Typically,  
between 15 and 30 channels about 1 mm in diameter and  
preferably several millimeters deep are formed with a  
10    laser in the wall of the left ventricle to perfuse the  
heart muscle with blood coming directly from the inside  
of the left ventricle, rather than traveling through  
the coronary arteries. Commonly assigned U.S. Patent  
No. 5,910,150 to Saadat describes mechanical apparatus  
15    for forming such channels. PCT Publication WO 98/17186  
describes a laser-based system for performing PMR that  
includes needle adjacent to the laser element for  
injecting a contrast agent to mark the position of the  
PMR channels for imaging.

20               U.S. Patent No. 5,840,059 to March et al.  
describes a laser-based PMR system that deposits a  
angiogenic agent, such as a gene vector or genetically  
engineered harvested cells, into the channel formed  
during the PMR procedure to promote angiogenesis. A  
25    drawback of this approach, however, is that blood  
pulsing through the PMR channel during normal cardiac  
wall motion may cause the angiogenic factor to be  
promptly washed out of the channel, thereby dissipating  
any beneficial effect obtainable from its introduction.  
30    In addition, it is relatively difficult and expensive  
to use engineer and produce the kinds of angiogenic  
factors referred to in the foregoing patent.

              Accordingly, it would be desirable to provide  
apparatus and methods for delivering angiogenic agents  
35    in conjunction with PMR treatments that promote long-  
term residence of the angiogenic agent in the vicinity  
of the treated tissue. It further would be desirable  
to provide relatively low-cost and readily available or

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5 readily prepared angiogenic agents for use in  
conjunction with PMR.

Wartiovaara et al., "Peripheral Blood  
Platelets Express VEGF-C and VEGF which Are Released  
During Platelet Activation," Thromb Haemost, 80:171-175  
10 (1998), describes that a variety of vascular  
endothelial growth factors (VEGF) may be derived from  
platelets. Knighton et al., "Role of Platelets and  
Fibrin in the Healing Sequence," Ann. Surg., 196(4)379-  
388 (1982), which is incorporated herein by reference,  
15 describes that thrombin-activated platelets, when  
injected in vivo in rabbit corneas, produced  
neovascularization that was dose related. U.S. Patent  
Nos. 4,957,742 to Knighton, U.S. Patent No. 4,479,896  
to Antoniades, and U.S. Patent No. 5,834,418 to Brazeau  
20 describe methods of extracting platelet growth factors  
from blood.

Sakai et al., "Autologous Cardiomyocyte  
Transplantation Improves Cardiac Function After  
Myocardial Injury," presented at the 1999 STS  
25 Convention, San Antonio, New Mexico, January 1999,  
suggests that autologous cardiomyocytes may be  
harvested, cultured and re-injected into injured  
myocardium to restore ventricular function.

In view of the foregoing, it would be  
30 desirable to provide apparatus and methods for using  
autologous materials in conjunction with PMR to augment  
angiogenesis resulting from forming myocardial  
channels.

It further would be desirable to provide  
35 apparatus and methods that reduce the risk of such  
autologous angiogenic materials from washing out of the  
PMR channels, and instead promote retention of such  
materials by injecting the angiogenic materials into

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5 the myocardium adjacent to the PMR channels.

#### Summary Of The Invention

In view of the foregoing, it is an object of this invention to provide apparatus and methods for  
10 delivering angiogenic agents in conjunction with PMR treatments that promote long-term residence of the angiogenic agent in the vicinity of the treated tissue.

It is another object of the present invention to provide apparatus and methods for conveniently and  
15 economically preparing autologous angiogenic agents for use in conjunction with PMR.

It is another object of this invention to provide apparatus and methods for using autologous materials in conjunction with PMR to augment  
20 angiogenesis resulting from forming myocardial channels.

It is also an object of the present invention to provide apparatus and methods that reduce the risk of such autologous angiogenic materials from washing  
25 out of the PMR channels, and instead promote retention of such materials.

It is a further object of the present invention to provide apparatus and methods for performing percutaneous myocardial revascularization  
30 that enable autologous angiogenic agents, such as platelets, platelet derived growth factors or cardiomyocytes to be injected into the myocardium adjacent to the PMR channels.

These and other objects of the present  
35 invention are accomplished by providing methods for collecting and processing autologous biological materials to form autologous angiogenic agents. Apparatus and methods also are provided for performing percutaneous myocardial revascularization that includes

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5 an injection needle disposed in spaced-apart relation to the channel-forming tool, so that a predetermined amount of the autologous angiogenic agent may be injected into the myocardium adjacent to the PMR channel.

10 In accordance with the principles of the present invention, blood, cardiomyocytes, or other biological material is first collected from a patient scheduled to undergo PMR. The biological material is then treated to concentrate and activate or express one  
15 or more platelet derived growth factors, and is stored in preparation for re-injection into the patient's myocardium during a PMR procedure.

• Apparatus suitable for implementing the methods of the present invention comprises a catheter  
20 having an end region that is directable to contact a patient's endocardium at a plurality of positions. Preferably, the catheter comprises inner and outer catheters each having preformed distal bends, so that the distal end of the inner catheter is directable to a  
25 plurality of positions. A cutting head is disposed within a lumen of the inner catheter and coupled to a drive tube that rotates and reciprocates the drive shaft. The drive tube is coupled to a motor that imparts rotational motion to the drive tube. The  
30 cutting head and drive tube include a lumen through which severed tissue is aspirated.

One or more stabilizing elements, are disposed on the distal end to retain the inner catheter in position while the cutting head is reciprocated  
35 beyond a distal endface of the inner catheter. In accordance with the present invention, the stabilizing elements also serve as injection needles for the re-injecting autologous angiogenic agent into the

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5 patient's myocardium in the vicinity of the channels formed by the cutting head. Methods of using the apparatus to deliver angiogenic agents also are described.

10 Brief Description Of The Drawings

Further features of the invention, its nature and various advantages will be more apparent from the accompanying drawings and the following detailed description of the preferred embodiments, in which:

15 FIG. 1 is a flow chart illustrating steps of collecting and processing blood to prepare autologous angiogenic agents;

FIG. 2 is a flow chart for an alternative method of the present invention wherein cardiomyocytes are collected and processed for re-injection into a patient's myocardium;

25 FIG. 3 is an illustrative view of a distal end of apparatus of the present invention injecting boluses of autologous angiogenic material adjacent to channels formed by the device;

FIG. 4 is a perspective view of an illustrative embodiment of apparatus suitable for implementing the methods of the present invention;

30 FIG. 5 is a partial sectional view of the distal region of the apparatus of FIG. 1;

FIG. 6 is a perspective view illustrating how the inner and outer catheters can be rotated to position the distal end of the inner catheter at a plurality of positions;

35 FIGS. 7A and 7B are, respectively, a perspective view and sectional view of an illustrative handle of the apparatus of FIG. 4;

FIG. 8 is a block diagram of the components of a controller constructed in accordance with the

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5 present invention; and

FIGS. 9A-9C are views illustrating deployment and use of the apparatus of FIG. 3 to percutaneously form channels in the myocardium and inject autologous angiogenic agents.

10

#### Detailed Description Of The Invention

The present invention provides methods for collecting and preparing autologous biological materials to form angiogenic agents, and apparatus for  
15 injecting those angiogenic agents into a patient's myocardium in the vicinity of channels formed by PMR. In accordance with the methods of the present invention, a series of channels is cut into the myocardium using a rotating cutting head through which  
20 severed material is aspirated. A stabilizer element fixed in a spaced-apart relation to the cutting head is employed to inject the autologous angiogenic material into pockets in the vicinity of the PMR channel. Advantageously, the angiogenic material disposed within  
25 pockets may migrate to towards the PMR channels to enhance revascularization, without being washed out of the PMR channel as in previously known methods.

Referring to FIG. 1, a first illustrative method of providing autologous angiogenic agents is  
30 described. A patient scheduled for a PMR procedure arranges to visit the hospital or clinic where the procedure is to be performed several days in advance of the procedure, and a quantity of whole blood is collected at step 10.

35 At step 11, the blood is then centrifuged using any of a number of previously known techniques, e.g., such as described in the foregoing patent to Knighton, to obtain a platelet rich plasma. The resulting platelet-rich plasma may be further



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5 centrifuged, and the platelet concentrate resuspended  
in a buffered solution to a concentration of about a  
million platelets per milliliter or less.

At step 12, the platelets are activated using  
one of a number of known techniques, and preferably by  
10 being exposed to thrombin about 1 to 10 units of  
purified thrombin per ml of resuspended platelet  
material, again as described in the above-incorporated  
article by Knighton. At step 13, the resulting  
angiogenic agent is filled in appropriately sized vials  
15 for use in conjunction with the patient's PMR procedure  
and stored under refrigeration, until the day of the  
PMR procedure.

Other methods for preparing an angiogenic  
agent from the patient's blood also may be employed, as  
20 described in the above-referenced articles. It is  
sufficient for the method illustrated in FIG. 1 that,  
at the end of the collection and processing step, an  
angiogenic platelet-rich agent has been prepared, at a  
much lower cost than associated with the production of  
25 gene vectors such as described in the aforementioned  
March et al. patent.

Referring to FIG. 2, an alternative method of  
collecting and preparing an autologous angiogenic agent  
is described. In this method, prior to the date of a  
30 scheduled PMR procedure, the patient arranges to visit  
the hospital or clinic to have a number of cells  
harvested. For example, using the PMR device described  
in the aforementioned patent to Saadat, which is  
incorporated herein by reference, a quantity of  
35 myocardial cells may be harvested, at step 21.  
Alternatively, other suitable cells, such as bone  
marrow cells, may be extracted.

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5           At step 22, the harvested cells are processed and prepared for use in conjunction with the subsequent PMR procedure. For example, the harvested cells may be cultured, using techniques which are per se known and described in the above-mentioned work of Sakai. At  
10   step 23, the harvested cells are then divided and suspended in an appropriately buffered solution. The resulting angiogenic agent is filled in appropriately sized vials and stored awaiting re-injection during the PMR procedure.

15           Referring now to FIG. 3, illustrative methods of injecting an autologous angiogenic agent in conjunction with PMR are described. In FIG. 3, distal end 30 of PMR apparatus, as described hereinbelow, is disposed adjacent to endocardium E in a patient's left  
20   ventricle. Reciprocable cutting head 31 of the PMR apparatus is used to bore channels C into myocardium M through the endocardial surface.

          In accordance with the methods of the present invention, hollow reciprocable stabilizer needle 32 is  
25   used to inject a bolus of a predetermined quantity of autologous angiogenic agent into "pocket" P adjacent to channel C upon completion of the channel-forming operation of cutting head 31. Advantageously, the angiogenic agent is expected to migrate from the pocket  
30   P towards the channel over a period of time, thereby enhancing revascularization, but without having the angiogenic agent washed out of the channel during normal wall motion.

          Referring now to FIGS. 4 and 5, illustrative  
35   apparatus 40 suitable for practicing the methods of the present invention is described. Apparatus 40 includes device 41 comprising handle 44 having inner catheter 43 disposed within outer guide catheter 42, and coupled to

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5 controller 45 via cable 46 and vacuum hose 47. Cutting head 48 having lumen 49 and sharpened distal end 50 is disposed within lumen 51 of inner catheter 43. Cutting head 48 is coupled to drive tube 52, which in turn is coupled via cable 46 to a drive system contained in  
10 controller 45 that imparts rotational and longitudinal motion to drive tube 52 and cutting head 48. Suction is drawn through lumen 49 of cutting head 48 and drive tube 52 to aspirate tissue severed by the cutting head to tissue trap 53 connected to controller 45 via vacuum  
15 hose 47.

Controller 45 comprises a vacuum pump or vacuum canister (not shown) that draws suction through lumen 54 of drive tube 52 via hose 47, a drive train (not shown) including a motor and gearing that impart  
20 rotational motion to drive tube 52 via cable 46, and a linear actuator mechanism (e.g., electromechanical or pneumatic) that reciprocates drive tube 52 and cutting head 48 within lumen 51 of inner catheter 43. Controller 45 also includes display panel 55, input  
25 panel 56 (e.g., a plurality of selector switches) and circuitry (see FIG. 7) for controlling operation of device 41. Further details of controller 45 are described in the above-incorporated patent to Saadat.

Inner catheter 43 is disposed for movement,  
30 either rotational, longitudinal or both, within lumen 57 of outer guide catheter 42. Inner catheter 43 further includes lumen 58 through which hollow needle stabilizer 59 may be reciprocated from a retracted position, within lumen 58, to an extended position,  
35 extending beyond distal endface 60 of inner catheter 43 (as shown in FIG. 5). A proximal end of hollow needle stabilizer 59 is coupled to slider button 61 of handle 44. When moved to the extended position, needle

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5 stabilizer 59 retains the distal end of inner catheter 43 in position with respect to an endocardial surface, and counteracts reaction forces generated when cutting head 48 is actuated.

10 Cutting head 48 and drive tube 52 are coupled via cable 46 to a drive train that moves cutting head 48 from a retracted position within lumen 51 of inner catheter 43 (as shown in FIG. 5), to an extended position wherein cutting head 48 and a distal portion of drive tube 52 extend beyond distal endface 60 (see  
15 FIG. 6). Button 62 of handle 44 signals controller 45 to extend and rotate cutting head 48 to cut a channel in the myocardium. Myocardial tissue severed by cutting head 48 is aspirated through lumen 54 of drive tube 52 to tissue trap 53 to reduce the risk that the  
20 severed tissue will embolize. Cutting head 48 preferably is constructed of a radio-opaque material or includes band 65 of radio-opaque material, such as platinum-iridium, disposed on its proximal end to assist in visualizing the location of the cutting head  
25 under a fluoroscope.

Referring to FIG. 6, outer guide catheter 42 and inner catheter 43 preferably include preformed bends. In particular, by rotating outer guide catheter 42 (indicated by arrows A) or inner catheter 43 (as  
30 indicated by arrows B) relative to one another, or extending inner catheter 43 longitudinally with respect to outer guide catheter 42 (as indicated by arrows C), distal endface 60 of inner catheter 43 may be disposed at a plurality of tissue contacting locations.  
35 Accordingly, outer guide catheter may disposed at a first orientation relative to an endocardial surface, and then inner catheter 43 may be moved relative to outer catheter 42 to form channels at a plurality of

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5 positions along the path indicated by arrows B. Outer catheter 42 may then be moved along the path indicated by arrows A, and a new series of holes may then be formed at that position by further rotating inner catheter 43. As will of course be understood, needle stabilizer 59 and cutting head 48 are retracted when  
10 moving between one channel forming position and another.

Referring now to FIGS. 7A and 7B, an illustrative arrangement of the components of handle 44  
15 is described. Handle 44 comprises proximal and distal portions 70 and 71, respectively, joined so that distal portion 71 may be rotated independently of proximal portion 70. Proximal portion 70 is coupled to cable 46 and includes button 62 for activating the cutting head  
20 to bore a channel. Distal portion 71 is affixed to inner catheter 43 so that rotation of knob 63 of portion 71 is transmitted to the distal end of inner catheter 43.

Slider button 61 is coupled to needle  
25 stabilizer 59, so that movement of button 61 in the distal direction deploys needle stabilizer 59, and movement of button 61 in the proximal direction retracts needle stabilizer 59 within lumen 58 of inner catheter 43. Needle stabilizer 59 includes a lumen  
30 through which the autologous angiogenic agent is injected, as described hereinabove, for example, by depressing button 61. Wheel 64, if provided, is coupled to inner catheter 43 to permit optional adjustment of the cutting depth attained by cutting  
35 head 48.

With respect to FIG. 7B, wheel 64 is disposed within tubular member 76 and extends within portions 70 and 71. Inner catheter 43 is coupled to a rigid

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5 tubular member (e.g., stainless steel hypotube) that  
extends through element 77. Element 77 in turn is  
coupled through tubular member 78 to distal portion 71,  
so that rotation of distal portion 71 is transmitted to  
inner catheter 43. Tubular member 76 is coupled by  
10 threads to tubular member 78 so that rotation of wheel  
64 causes inner catheter to be moved in a distal or  
proximal direction relative to drive tube 52 (depending  
upon direction of rotation), thereby lengthening or  
shortening the stroke of cutting head 48 beyond distal  
15 endface 60 of the inner catheter.

Drive tube 52 has proximal end 80 affixed to  
tubular member 81 having skive 82. Tubular member 81  
is coupled to drive wire 83. Tubular member 81 is  
disposed for rotational and longitudinal motion,  
20 imparted by drive wire 83, within tubular member 84.  
The distal end of tubular member 84 is disposed within  
tubular member 78, while the proximal end includes a  
suitable bearing that seals against tubular member 81  
without binding. Tissue passing through lumen 54 of  
25 drive tube 52 exits through skive 82 into the interior  
of tubular member 84, and then aspirated through port  
85 into vacuum hose 47. Tubular member 84 is affixed  
to the interior of proximal portion 71 by element 86,  
which also supports button 62. Needle stabilizer 59 is  
30 fastened to slider button 61, which is in turn coupled  
to spool 77 to provide rigidity to the assembly.  
Needle stabilizer also includes a port that permits the  
lumen of the needle to be coupled to a vial or syringe  
containing autologous angiogenic agent.

35 Handle 44 therefore provides the ability to  
rotate distal portion 71 of the handle to orient the  
bend in inner catheter 43, while retaining button 62 on  
top of proximal portion 70 facing upward. Slider

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5 button 61 permits needle stabilizer 59 to be  
selectively deployed, and knob 63 permits the inner  
catheter to be rotated relative to the outer guide  
catheter. Wheel 64 permits the inner catheter to be  
translated distally or proximally with respect to the  
10 cutting head, to account for the effects of inserting  
the distal portion of device 41 along a tortuous path.

With respect to FIG. 8, a block diagram of  
the components of controller 45 are described.  
Controller 45 preferably comprises microprocessor 90  
15 coupled to display panel 55, input device 56 (e.g.,  
keyboard), activation button 62 of handle 44, data  
storage 91 (e.g., RAM and ROM or hard disk), vacuum  
pump 92, linear actuator mechanism 93 (e.g., a worm  
screw drive or pneumatic cylinder), motor 94 and  
20 monitoring circuitry 95. Monitoring circuitry 95 may  
be coupled to components 92-94, for example, to monitor  
the level of vacuum drawn by vacuum pump 92, or a motor  
parameter, such as the displacement of or linear force  
applied by linear actuator mechanism 93 and/or the  
25 speed of or electrical current drawn by motor 94.

For example, monitoring circuitry 95 may be  
arranged to ensure that the cutting head is not  
extended unless there is an appropriate level of  
suction being drawn through drive tube 52 and cutting  
30 head 48, or that the cutting head is rotating at a  
desired RPM before being advanced into tissue.  
Additional applications for monitoring circuitry 95 are  
described in the above-incorporated, commonly assigned  
U.S. patent.

35 Referring now to FIGS. 9A-9C, a method of  
using the apparatus of the present invention perform  
PMR and to inject autologous angiogenic agents is  
described. In FIG. 9A, distal region 100 of device 41

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5 of FIG. 1 is shown positioned in a patient's left  
ventricular cavity, using techniques which are per se  
known. Specifically, distal region 100 of device 41 is  
inserted via a femoral artery, and is maneuvered under  
fluoroscopic guidance in a retrograde manner up through  
10 the descending aorta, through aortic arch **A**, and down  
through ascending aorta **AA** and aortic valve **AV** into  
left ventricle **LV**. Previously known imaging  
techniques, such as ultrasound, MRI scan, CT scan, or  
fluoroscopy, may be used to verify the location of the  
15 distal region 100 within the heart.

In FIG. 9B, slider button 61 on handle 44 is  
advanced to extend needle stabilizer 59 so that it  
penetrates into the myocardium a predetermined  
distance, for example, 7 mm. Button 62 on handle 44  
20 then is depressed, causing the drive system of  
controller 45 to extend cutting head 48 to bore a  
channel into the myocardium to a predetermined depth.  
Alternatively, button 62 of handle 44 may be omitted,  
and controller 45 instead programmed so that linear  
25 actuator 93 causes the cutting head to be extended a  
predetermined interval of time (e.g., 1 second) after  
slider button 61 is actuated. In this alternative  
embodiment, slider button 61 will of course have to  
generate a signal that is communicated to controller 45  
30 via cable 46.

When cutting head 48 engages the endocardium,  
a reaction force is generated in inner catheter 41 that  
tends both to push distal region 100 away from the  
tissue. Needle stabilizer 59 counteracts these  
35 reaction forces and reduces transverse movement of the  
distal end of inner catheter 43, thus retaining the  
inner catheter in position while the cutting head is  
extended and retracted. Tissue severed by the cutting



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5 head is aspirated to trap 53 of controller 45.

Once cutting head reaches its maximum extension, as determined by any of the means described hereinabove, processor 90 causes forward motion of the cutting head to cease. In the embodiments using linear  
10 actuator 93, processor 90 also issues a command to reverse the direction of linear actuator 93. This in turn causes cutting head 48 to be withdrawn from channel C formed in the myocardium to a position just below distal endface 60 of inner catheter 43. Button  
15 61 is then depressed to inject a bolus of autologous angiogenic agent into the myocardium at a location adjacent to channel C.

Advantageously, the needle stabilizer of device 41 permits an angiogenic agent to be injected at  
20 a location a predetermined distance from the channel formed by cutting head 48. By comparison, use of a separate needle catheter to inject an angiogenic agent into the myocardium after the channel forming process is completed would result in the angiogenic agent being  
25 injected at random locations relative to the previously formed channels.

As shown in FIG. 9C, a matrix of spaced-apart channels C and associated pockets of angiogenic agent may be formed in the wall of left ventricular wall LV  
30 by rotating outer guide catheter 42 and inner catheter 43 relative to one another (see FIG. 6). Needle stabilizer 59 and cutting head 48 are then advanced at each position to form further channels C in the tissue. The foregoing methods therefore enable a matrix of  
35 channels to be formed in the left ventricular wall. It is believed that such channels may be drilled anywhere on the walls of the heart chamber, including the septum, apex and left ventricular wall, and the above-

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5   described apparatus provides this capability.

          While preferred illustrative embodiments of  
the invention are described, it will be apparent that  
various changes and modifications may be made therein  
without departing from the invention, and the appended  
10   claims are intended to cover all such changes and  
modifications that fall within the true spirit and  
scope of the invention.

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What Is Claimed Is:

1. A method of performing percutaneous myocardial revascularization of a patient comprising:
  - collecting autologous biological material from the patient;
  - preparing the autologous biological material to form an angiogenic agent;
  - providing a catheter adapted for insertion into the left ventricle comprising a hollow stabilizer element and a cutting head movable from a retracted position to an extended position;
  - advancing a distal region of the catheter transluminally to a position within the patient's left ventricle;
  - deploying the stabilizer element to stabilize the distal region of the catheter in contact with an endocardial surface;
  - advancing the cutting head from the retracted to the extended position to bore a channel into the patient's cardiac tissue; and
  - injecting an amount of the angiogenic agent through the hollow stabilizer needle into a region of the patient's cardiac tissue adjacent to the channel.
2. The method of claim 1 wherein the stabilizer element comprises a first retractable needle and deploying the stabilizer element comprises advancing the retractable needle to penetrate into the patient's cardiac tissue.
3. The method of claim 1 wherein collecting autologous biological material from the patient comprises collecting a quantity of whole blood from the patient.

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4. The method of claim 1 wherein preparing the autologous biological material comprises centrifuging the whole blood to form a platelet-rich plasma.

5. The method of claim 4 wherein preparing the autologous material further comprises activating the platelet rich plasma.

6. The method of claim 5 wherein activating the platelet rich plasma further comprises activating the platelet rich plasma with purified thrombin.

7. The method of claim 1 wherein collecting autologous biological material from the patient comprises harvesting cells from the patient's cardiac tissue or bone marrow.

8. The method of claim 7 wherein preparing the autologous material further comprises culturing the harvested cells in vitro.

9. The method of claim 1 further comprising aspirating cardiac tissue severed by the cutting head.

10. The method of claim 1 further comprising, after the step of preparing an angiogenic agent, storing the angiogenic agent under refrigeration.

11. A method of performing percutaneous revascularization of a patient's cardiac tissue, the method comprising:

collecting autologous biological material

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from the patient;

preparing the autologous biological material to form an angiogenic agent;

providing a catheter adapted for insertion into the left ventricle comprising a hollow needle movable from a retracted position to an extended position and a cutting head movable from a retracted position to an extended position;

advancing a distal region of the catheter transluminally to a position within a patient's left ventricle;

advancing the hollow needle to the extended position to penetrate and stabilize the distal region of the catheter in contact with an endocardial surface;

rotating the cutting head;

advancing the cutting head from the retracted to the extended position to bore a channel into the patient's cardiac tissue; and

injecting an amount of the angiogenic agent through the hollow needle into a region of the patient's cardiac tissue adjacent to the channel.

12. The method of claim 11 wherein injecting an amount of the angiogenic agent comprises injecting a predetermined bolus of angiogenic agent to form a pocket of angiogenic material adjacent to the channel.

13. The method of claim 11 wherein collecting autologous biological material from the patient comprises collecting a quantity of whole blood from the patient.

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14. The method of claim 11 wherein preparing the autologous biological material comprises centrifuging the whole blood to form a platelet-rich plasma.

15. The method of claim 14 wherein preparing the autologous material further comprises activating the platelet rich plasma.

16. The method of claim 15 wherein activating the platelet rich plasma further comprises activating the platelet rich plasma with purified thrombin.

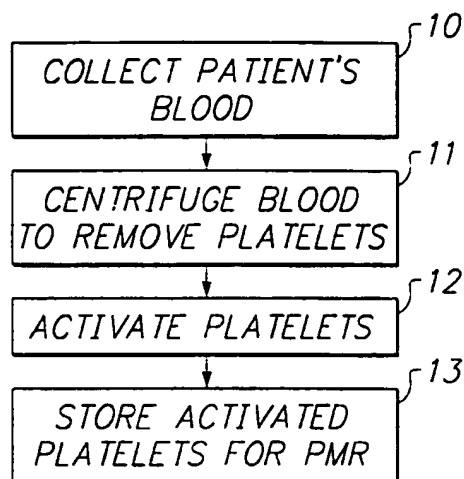
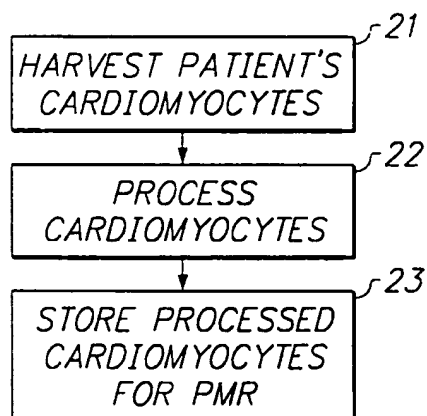
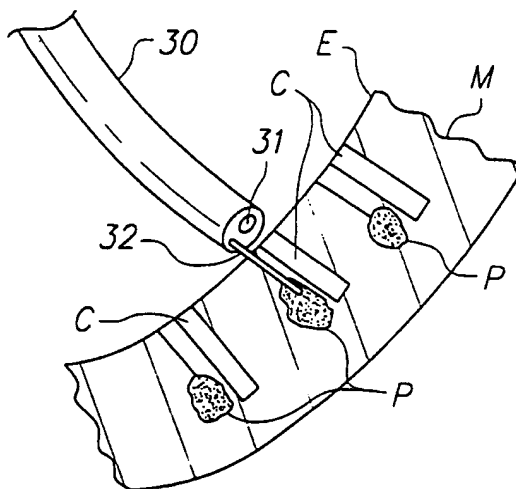
17. The method of claim 11 wherein collecting autologous biological material from the patient comprises harvesting cells from the patient's cardiac tissue or bone marrow.

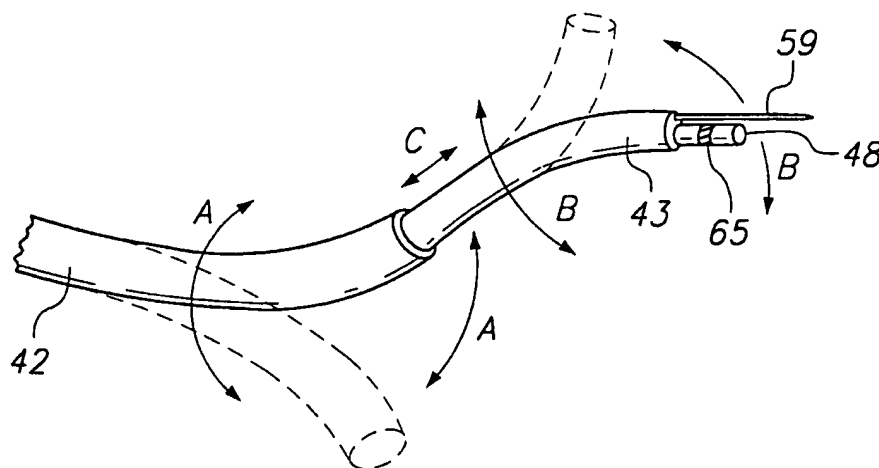
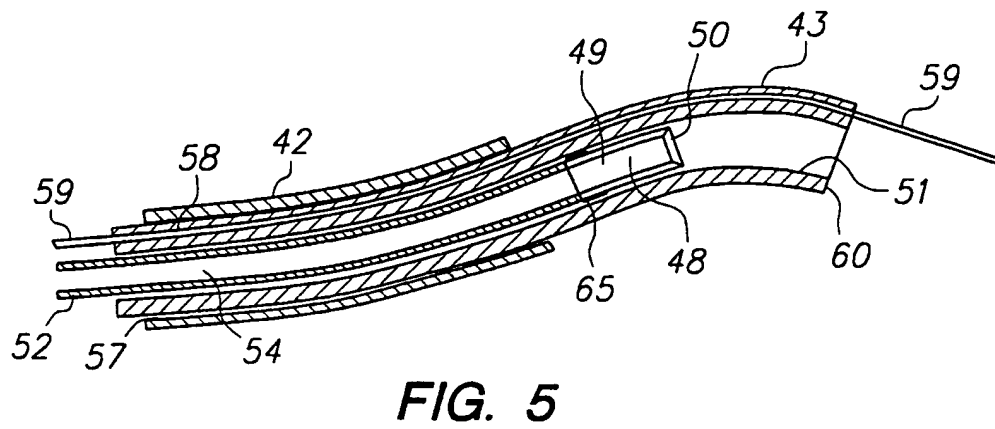
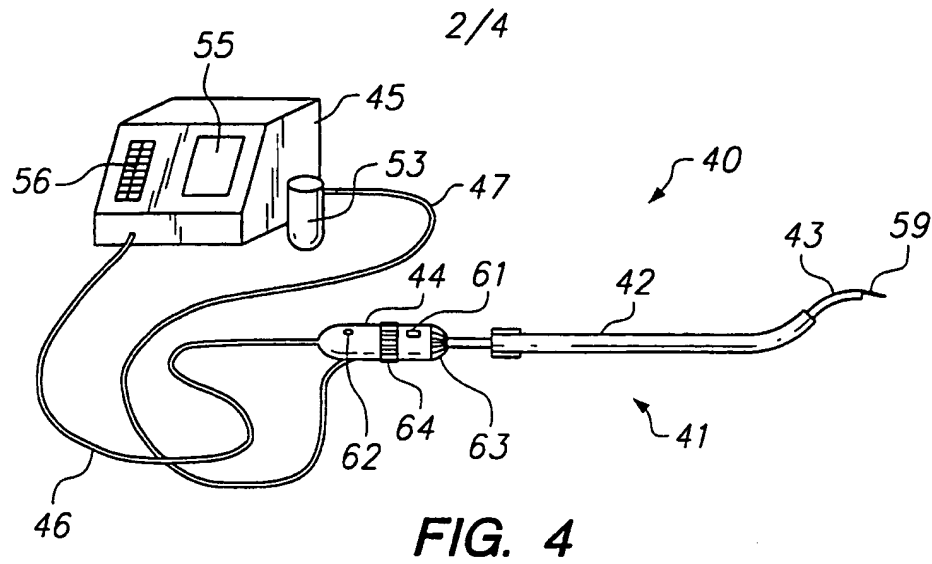
18. The method of claim 17 wherein preparing the autologous material further comprises culturing the harvested cells in vitro.

19. The method of claim 11 further comprising aspirating cardiac tissue severed by the cutting head.

20. The method of claim 1 further comprising, after the step of preparing an angiogenic agent, storing the angiogenic agent under refrigeration.

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**FIG. 1****FIG. 2****FIG. 3**





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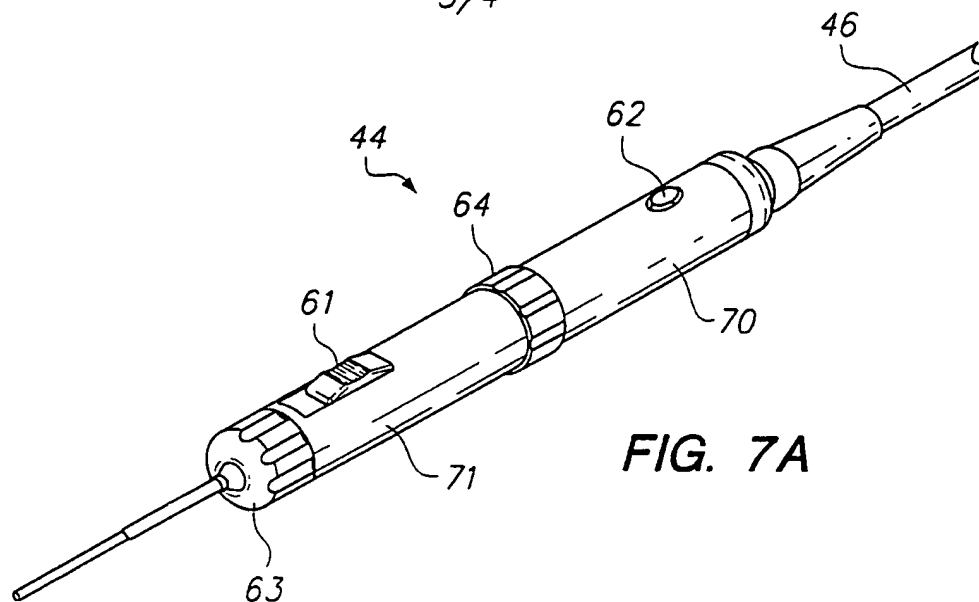


FIG. 7A

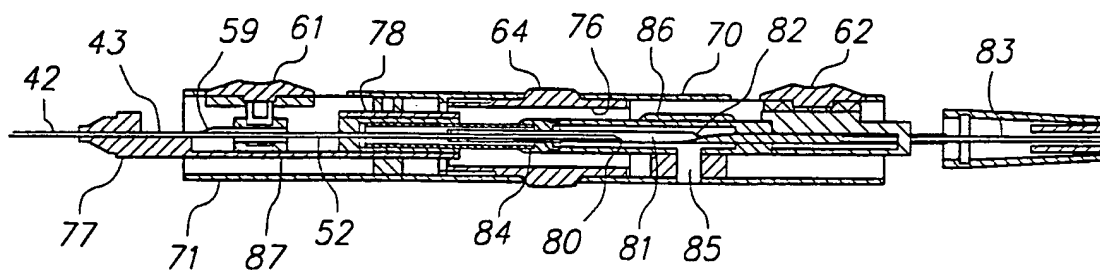


FIG. 7B

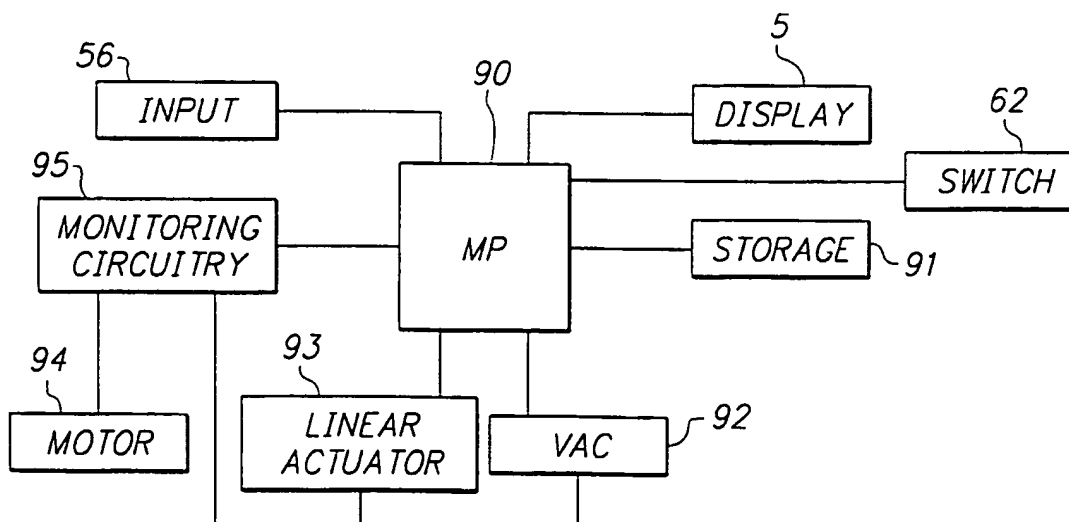
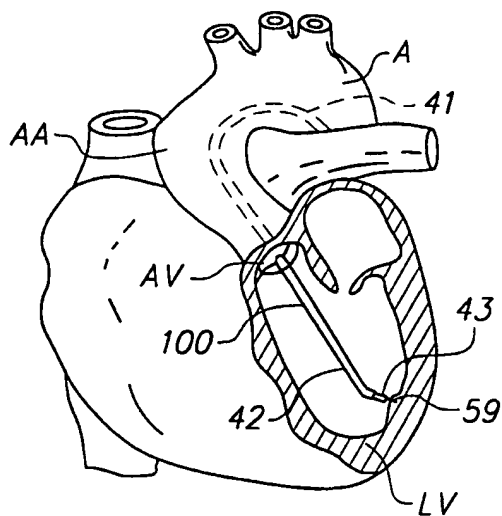
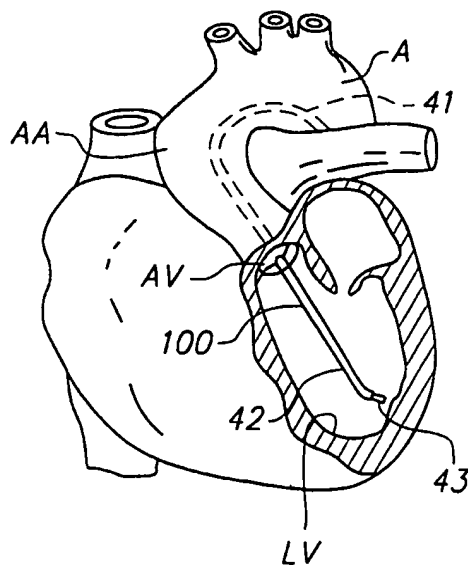


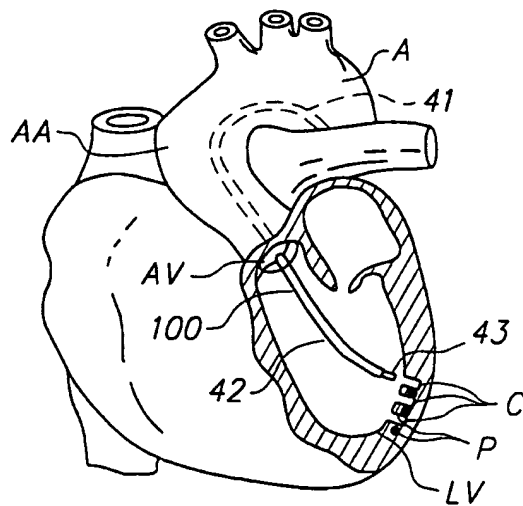
FIG. 8

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**FIG. 9A**



**FIG. 9B**



**FIG. 9C**

## INTERNATIONAL SEARCH REPORT

International application No.  
PCT/US00/07274

## A. CLASSIFICATION OF SUBJECT MATTER

IPC(7) :A61B 17/00

US CL :606/170

According to International Patent Classification (IPC) or to both national classification and IPC

## B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

U.S. : 606/1, 14, 46, 108, 159, 167, 170, 180

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

## C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	WO 96/35469 A (KESTEN et al.) 14 November 1996, entire document.	1-20



Further documents are listed in the continuation of Box C.



See patent family annex.

* Special categories of cited documents:	"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
"A" document defining the general state of the art which is not considered to be of particular relevance	"X" document of particular relevance, the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
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"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)	"&" document member of the same patent family
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"P" document published prior to the international filing date but later than the priority date claimed	

Date of the actual completion of the international search

04 MAY 2000

Date of mailing of the international search report

08 JUN 2000

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